

Modified-CS: modifying Compressive Sensing for problems with partially known support

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The Problem

- ▶ Reconstruct an m -length sparse vector, x , from an n -length measurement vector, $y := Ax$, when $n < m$
 - ▶ *use partial knowledge of the support of x to reduce the n required for exact reconstruction*
- ▶ Support of x is $N = T \cup \Delta \setminus \Delta_e$
 - ▶ T : “known” part of the support
 - ▶ Δ : “unknown” part of the support, Δ is disjoint with T
 - ▶ $\Delta_e \subseteq T$: error in the known part
- ▶ Measurement matrix, A , satisfies the S -RIP, $S = |T| + 2|\Delta|$

Application - 1: single signal/image

- ▶ T known from prior knowledge,
- ▶ e.g. in a natural image (often wavelet-sparse) with a small black background, most approximation (lowest subband) coeff's will be nonzero
- ▶ Set $T = \{\text{indices of all approximation coeff's}\}$, then
 - ▶ $\Delta_e = \{\text{indices of approximation coeff's which are zero}\}$
 - ▶ $\Delta = \{\text{indices of scaling coeff's which are nonzero}\}$

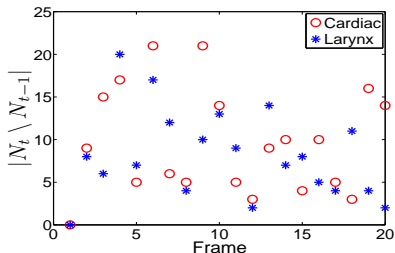
Application - 2: time sequence of signals/images

- ▶ Recursively reconstruct a time sequence of sparse vectors, x_t , with support, N_t , from measurement vectors, $y_t := Ax_t$
 - ▶ “recursively”: use only \hat{x}_{t-1} and y_t to reconstruct x_t
- ▶ Applications: real-time dynamic MRI, single-pixel video, ...
 - ▶ *use: the sparsity pattern of the signal sequence changes slowly*
- ▶ Set $T = \hat{N}_{t-1}$ (support estimate from $t - 1$)

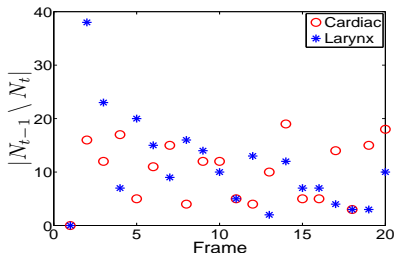
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- ▶ Applications: real-time dynamic MRI, single-pixel video, ...
 - ▶ *use: the sparsity pattern of the signal sequence changes slowly*
- ▶ Set $T = \hat{N}_{t-1}$ (support estimate from $t - 1$)
 - ▶ if $\hat{N}_{t-1} = N_{t-1}$ (exact recon), $\Delta = N_t \setminus N_{t-1}$, $\Delta_e = N_{t-1} \setminus N_t$
 - ▶ slow changes in sparsity pattern $\iff |\Delta|, |\Delta_e| \ll |N_t| \approx |T|$

Example: slow support change of medical image seq's



(a) additions: $|N_t \setminus N_{t-1}|$



(b) deletions: $|N_{t-1} \setminus N_t|$

- ▶ N_t : 99%-energy support of 2D-DWT of image
- ▶ **Maximum size of addition or deletion less than $|N_t|/50$ for both**
 - ▶ heart: $|N_t| \approx 1400 - 1500$, $m = 4096$
 - ▶ larynx: $|N_t| \approx 4400 - 4600$, $m = 65536$

Outline

Background and the proposed solution (modified-CS)

Exact reconstruction result

Simulation results

Summary, Related work and Future work

Notation, Recap of Compressive Sensing [Donoho'05, Candes, Romberg, Tao'05]

▶ Notation:

- ▶ A_T : sub-matrix containing columns of A with indices in set T
- ▶ β_T : sub-vector containing elements of β with indices in set T
- ▶ $T^c = [1 : m] \setminus T$: complement of set T
- ▶ $\|A\|$: spectral matrix norm (induced 2-norm)
- ▶ A' : denotes the transpose of matrix A

- ▶ **Compressive Sensing:** Reconstructs a sparse signal, x , with support, N , from $y := Ax$ by solving

$$\min_{\beta} \|\beta\|_1 \text{ s.t. } y = A\beta$$

- ▶ Exact reconstruction will occur if $\delta_{2|N|} + \theta_{|N|,2|N|} < 1$

Define $\delta_S, \theta_{S,S'}$ [Candes,Romberg,Tao'05]

- ▶ Restricted isometry constant, δ_S : smallest real number s.t.

$$(1 - \delta_S) \|c\|_2^2 \leq \|A_T c\|_2^2 \leq (1 + \delta_S) \|c\|_2^2$$

\forall subsets T with $|T| \leq S$ and for all c

- ▶ easy to see: $\|(A_T' A_T)^{-1}\| \leq 1/(1 - \delta_{|T|})$

- ▶ Restricted orthogonality constant, $\theta_{S,S'}$: smallest real no. s.t.

$$|c_1' A_{T_1}' A_{T_2} c_2| \leq \theta_{S,S'} \|c_1\|_2 \|c_2\|_2$$

\forall disjoint sets T_1, T_2 with $|T_1| \leq S, |T_2| \leq S'$ and $\forall c_1, c_2$

- ▶ easy to see: $\|A_{T_1}' A_{T_2}\| \leq \theta_{|T_1|,|T_2|}$

Modified-CS [Vaswani, Lu, ISIT'09]

- ▶ Our problem: reconstruct x with support $N = T \cup \Delta \setminus \Delta_e$ from $y := Ax$ when T is known
- ▶ First consider the case: $|\Delta_e| = 0$, i.e. $N = T \cup \Delta$
 - ▶ among all solutions of $y = A\beta$, find the β whose support contains the smallest number of new additions to T

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$$\min_{\beta} \|(\beta)_{T^c}\|_0 \text{ s.t. } y = A\beta$$

- ▶ x is its unique solution if $\delta_S < 1$ for $S = |T| + 2|\Delta|$ (S-RIP)

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- ▶ *The above also holds when $|\Delta_e| \neq 0$, i.e. $N = T \cup \Delta \setminus \Delta_e$*
- ▶ Replace ℓ_0 norm by ℓ_1 norm: get a convex problem

$$\min_{\beta} \|(\beta)_{T^c}\|_1 \text{ s.t. } y = A\beta \quad \textbf{(modified-CS)}$$

Exact reconstruction using ℓ_0 modified-CS [Vaswani, Lu, ISIT'09]

$$\min_{\beta} \|\beta_{T^c}\|_0 \text{ s.t. } y = A\beta \quad (\ell_0 \text{ mod-CS})$$

- ▶ (ℓ_0 mod-CS) achieves exact reconstruction if
 - ▶ $\delta_{|T|+2|\Delta|} = \delta_{|N|+|\Delta_e|+|\Delta|} < 1$
 - ▶ if $|\Delta| = |\Delta_e| = |N|/50$, this becomes $\delta_{1.04|N|} < 1$

- ▶ Compare with CS
 - ▶ (ℓ_0 CS) needs $\delta_{2|N|} < 1$

recall: $T = N \cup \Delta_e \setminus \Delta$, T : known part of support, Δ : unknown part, Δ_e : error in known part

Exact reconstruction using modified-CS [Vaswani, Lu, ISIT'09]

$$\min_{\beta} \|\beta_{T^c}\|_1 \text{ s.t. } y = A\beta \quad (\text{mod-CS})$$

Theorem

x is the unique minimizer of (mod-CS) if $\delta_{|T|+|\Delta|} < 1$ and

$$\theta_{|\Delta|,|\Delta|} + \delta_{2|\Delta|} + \theta_{|\Delta|,2|\Delta|} + \delta_{|T|} + \theta_{|\Delta|,|T|}^2 + 2\theta_{2|\Delta|,|T|}^2 < 1$$

Corollary (simplified condition)

x is the unique minimizer of (mod-CS) if $|\Delta| \leq |T|$ and

$$\delta_{|T|+2|\Delta|} < 1/5$$

recall: $T = N \cup \Delta_e \setminus \Delta$, T : known part of support, Δ : unknown part, Δ_e : error in known part

Comparing modified-CS with CS

- ▶ Compare sufficient conditions for exact recon.

- ▶ *Modified-CS*: $\delta_{|T|+|\Delta|} < 1$ and

$$Mcond = (\delta_{2|\Delta|} + \theta_{|\Delta|,|\Delta|} + \theta_{|\Delta|,2|\Delta|}) + (\delta_{|T|} + \theta_{|\Delta|,|T|}^2 + 2\theta_{2|\Delta|,|T|}^2) < 1$$

- ▶ *CS* [Decoding by LP, Candes, Tao'05]:

$$Ccond = \delta_{2|N|} + \theta_{|N|,|N|} + \theta_{|N|,2|N|} < 1$$

- ▶ If $|\Delta| \approx |\Delta_e| \ll |N|$ (typical for medical image seq's),

$$Mcond \ll Ccond$$

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- ▶ $Mcond < 1$ can hold even with $n < 2|N|$

- ▶ In simulations with $n = 1.6|N|$:

- ▶ *Modified-CS worked w.p. 0.99* if $|\Delta| = |\Delta_e| = |N|/50$
- ▶ *CS worked w.p. 0*

Proof Idea: Lemma 1

- ▶ The idea of the proof is motivated by the proof of the exact reconstruction result for CS [Decoding by LP, Candes, Tao'05]

Lemma

x is the unique minimizer of (mod-CS) if $\delta_{|T|+|\Delta|} < 1$ and if we can find a vector w satisfying

- ▶ $A_T' w = 0$
- ▶ $A_\Delta' w = \text{sgn}(x_\Delta)$
- ▶ $\|A_{(T \cup \Delta)^c}' w\|_\infty < 1$

Proof Idea: Lemma 2

Lemma

Let c be a vector supported on a set T_d , that is disjoint with T , of size $|T_d| \leq S$, and let $\delta_S + \delta_{|T|} + \theta_{|T|,S}^2 < 1$.

Then there exists a vector \tilde{w} and an exceptional set, E , disjoint with $T \cup T_d$, of size $|E| < S'$ s.t. $\|\tilde{w}\|_2 \leq K_{|T|}(S)\|c\|_2$,

$$A_T' \tilde{w} = 0,$$

$$A_{T_d}' \tilde{w} = c,$$

$$\|A_E' \tilde{w}\|_2 \leq a_{|T|}(S, S')\|c\|_2,$$

$$\|A_{(T \cup T_d \cup E)^c}' \tilde{w}\|_\infty \leq \frac{a_{|T|}(S, S')}{\sqrt{S'}}\|c\|_2, \text{ where}$$

$$a_{|T|}(S, S') := \frac{\theta_{S',S} + \frac{\theta_{S',|T|} \theta_{S,|T|}}{1 - \delta_{|T|}}}{1 - \delta_S - \frac{\theta_{S,|T|}^2}{1 - \delta_{|T|}}}$$

Proof idea: Proving the result

- ▶ Apply Lemma 2 iteratively to find a w needed by Lemma 1
 - ▶ at iteration $k = 0$, apply it with $S = S' = |\Delta|$: get \tilde{w}_1
 - ▶ at iteration $k > 0$, apply it with $S = 2|\Delta|$, $S' = |\Delta|$: get \tilde{w}_{k+1}
 - ▶ define $w = \sum_k (-1)^{k-1} \tilde{w}_k$
 - ▶ can show that w satisfies $A_{\mathcal{T}'} w = 0$, $A_{\Delta'} w = \text{sgn}(x_{\Delta})$, and

$$\|A_{(\mathcal{T} \cup \Delta)^c} w\|_{\infty} < a_{|\mathcal{T}|}(2|\Delta|, |\Delta|) + a_{|\mathcal{T}|}(|\Delta|, |\Delta|)$$

- ▶ Thus if $a_{|\mathcal{T}|}(2|\Delta|, |\Delta|) + a_{|\mathcal{T}|}(|\Delta|, |\Delta|) < 1$, Lemma 1 applies

Simulation results: Probability of exact reconstruction

- ▶ fixed $m = 256$, $|N| = 0.1m$ (typical 99%-support size)
- ▶ used a random Gaussian A
- ▶ varied n (number of measurements), $|\Delta|$ and $|\Delta_e|$
 - ▶ for each choice, averaged over N , $(x)_N$, Δ , Δ_e

recall: n is number of measurements, Δ : unknown part of support, Δ_e : error in known part

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- ▶ For $n = 1.6|N|$,
 - ▶ CS works 0% times
 - ▶ Mod-CS works $\geq 99\%$ times if $|\Delta| \leq 0.04|N|$, $|\Delta_e| \leq 0.08|N|$

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- ▶ For $n = 2.5|N|$
 - ▶ CS works 0.2% times
 - ▶ Mod-CS works $\geq 99\%$ times if $|\Delta| \leq 0.20|N|$, $|\Delta_e| \leq 0.24|N|$

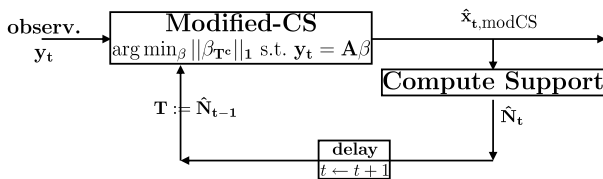
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- ▶ $n = 4|N|$: CS works 98% of times

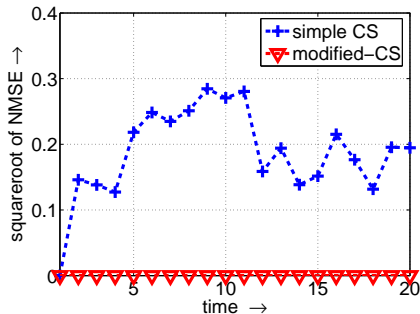
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Modified-CS for a time sequence of signals

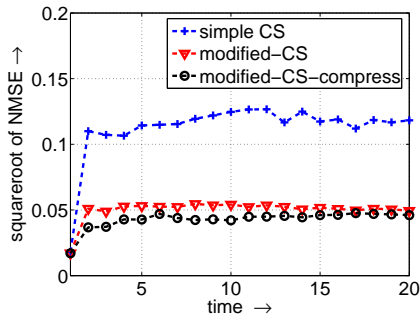


- Support computed as $\hat{N}_t = \{i \in [1 : m] : (\hat{x}_t)_i^2 > \alpha\}$

Simulated MRI: Reconstructing a cardiac image sequence



(c) $n = 0.16m$, Sparsified sequence



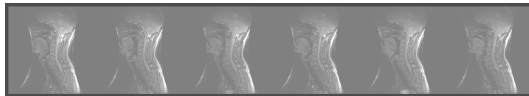
(d) $n = 0.19m$, True sequence

- ▶ sparsity basis: 2-level 2D-DWT, Daubechies-4 wavelet
- ▶ $m = 1024$ (32×32 image), $|N_t| \approx 107 \approx 0.1m$

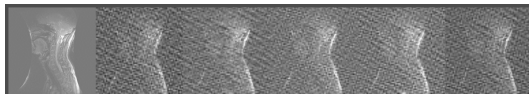
recall: n is number of measurements

Simulated MRI: Reconstructing a larynx image sequence

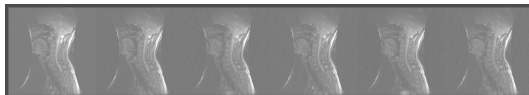
Original sequence



CS-reconstructed sequence



Modified CS reconstructed sequence



99%-energy support $|N_t| \approx 0.07m$, $|\Delta| \approx 0.001m$, $m = 65536$,
used $n = 0.16m$ (for $t > 0$), $n = 0.5m$ (for $t = 0$)

Summary

- ▶ Introduced modified-CS for sparse reconstruction problems with partially known support (known part may have error)
- ▶ Modified-CS solves

$$\min_{\beta} \|(\beta)_{T^c}\|_1 \text{ s.t. } y = A\beta$$

where T is the known part of the support

- ▶ Exact reconstruction if $|\Delta| \leq |T|$ and $\delta_{|T|+2|\Delta|} < 1/5$
- ▶ *Key app: recursive reconstruction of sparse signal sequences, e.g. real-time dynamic MRI, single-pixel video imaging,...*

Related work

- ▶ Similar problem to ours, do not study exact reconstruction
 - ▶ Least squares and Kalman filtered CS [Vaswani, ICIP'08, ICASSP'09]
 - ▶ Recursive lasso [Angelosante, Giannakis'09]
- ▶ Different problem than ours
 - ▶ Warm start and homotopy methods [Rozell et al'07, Asif, Romberg'09]
 - ▶ use previous recon. and/or homotopy methods to speed up the current optimization
 - ▶ *do not use the past to help reduce the number of measurements required for reconstructing the current signal*
 - ▶ Reconstruct a single signal from sequentially arriving measurements [Malioutov et al'08, Ghaoui NIPS'08, Asif, Romberg'09]
- ▶ Batch or Offline CS: [Wakin et al (video), Gamper et al (MRI), Jung et al (MRI)]

Ongoing and Future Work

- ▶ Modified-CS for noisy measurements (sparse KF) or compressible sequences and connections with KF

$$\min_{\beta} \gamma \|(\beta)_{T^c}\|_1 + \tilde{\gamma} \|(\beta)_T - (\hat{x}_{t-1})_T\|_2^2 + \|y_t - A\beta\|_2^2$$

- ▶ Stability for signal sequence recon from noisy measurements
 - ▶ for a given max. no. of additions per unit time, how slowly should they occur s.t. the error remains bounded at all times?
- ▶ Open-ended issues
 - ▶ handling deletions from support: currently only using heuristics
 - ▶ tight high probability bounds on n needed for modified-CS