

Introduction to Topics in Machine Learning

Namrata Vaswani

Department of Electrical and Computer Engineering
Iowa State University

- ▶ Compressed Sensing / Sparse Recovery: Given $y := Ax$ recover x from y when y is shorter than x . Use sparsity of x .
- ▶ Low-rank Matrix Completion: Given a subset of entries of a low-rank matrix M , complete the matrix
 - ▶ given $y = \mathcal{P}_\Omega(M)$, find M . Ω : set of indices of the observed entries
- ▶ Matrix Sensing: given a set of n linear functions of M , find M using the fact that M is low-rank
 - ▶ given $y = \mathcal{A}(M)$ where $\mathcal{A}(\cdot)$ is a linear operator, find M . This can be written as $y_i = \langle A_i, M \rangle$ where $\langle A, B \rangle = \text{trace}(A'B)$ is the usual inner product.
- ▶ Robust PCA: given $Y := X + L$, find X and L
 - ▶ L = unknown low rank matrix.
 - ▶ X = sparse matrix (corresponds to outliers)
- ▶ Phase retrieval: compute vector x from $y := |Ax|^2$. Here $|\cdot|$ means element-wise magnitude of the vector. More specifically $y_i = |A^i x|^2$ (here A^i is the i -th row of A).

- ▶ the term phase retrieval comes from Fourier imaging where A is the DFT matrix; but now it's used more generally for any matrix A
- ▶ Ranking and individualized ranking estimation

- ▶ CS: projection imaging - MRI, CT, single-pixel camera, radar, ...
- ▶ MC: recommendation system design, e.g., Netflix problem
- ▶ Matrix sensing: one special case is phase retrieval. Notice that we can rewrite $y_i = A^i x x' A^{i'} = \langle x x', A^i A^{i'} \rangle$
- ▶ RPCA: recommendation system design in the presence of outliers, Video analytics, Survey data analysis,
- ▶ Phase retrieval: astronomy, X-ray crystallography,...

Non-convex Problems: Alternating Minimization and Gradient Descent I

Alternating Min

- ▶ Goal: compute $\min_{x,y} f(x,y)$ when $f(\cdot)$ is non-convex
- ▶ Clearly $\min_{x,y} f(x,y) = \min_x(\min_y f(x,y))$ but of course in most cases, RHS is also hard to compute.
- ▶ Consider the class of problems where the min is easy when one variable is fixed, i.e., $\min_y f(x_0, y)$ is easy for a given x_0 and $\min_x f(x, y_0)$ is easy for a given y_0 .
 - ▶ A common solution: Alt-Min
 - ▶ Start with an initial guess x_0 .
 - ▶ Compute $y_1 \in \arg \min_y f(x_0, y)$
 - ▶ Compute $x_1 \in \arg \min_x f(x, y_1)$
 - ▶ Repeat above until a stopping criterion is met.
- ▶ Guarantees? Till very recently none. Recent work:

Non-convex Problems: Alternating Minimization and Gradient Descent II

- ▶ If initialized carefully, Alt-Min gets to within a small error of the true solution in a finite number of iterations. Possible to bound this number also.
- ▶ A common approach to initialization: “spectral method” - compute the top eigenvector of an appropriately defined matrix
- ▶ Guarantees exist for Matrix Completion and for Phase Retrieval

Gradient descent based approaches for non-convex problems

- ▶ With a suitable initialization, it is possible to get a guarantee
- ▶ Truncated gradient descent idea of “truncated Wirtinger flow” paper: the gradient turns out to be a weighted average of certain vectors; discard those weights that are too large and compute a truncated gradient estimate
- ▶

Old slides on sparse recovery

The sparse recovery / compressed sensing problem

- ▶ Given $y := Ax$ where A is a fat matrix, find x .
 - ▶ underdetermined system, without any other info, has infinite solutions
- ▶ Key applications where this occurs: Computed Tomography (CT) or MRI
 - ▶ CT: acquire radon transform of cross-section of interest
 - ▶ typical set up: obtain line integrals of the cross-section along a set of parallel lines at a given angle, and repeated for a number of angles from 0 to π), common set up: 22 angles, 256 parallel lines per angle
 - ▶ by Fourier slice theorem, can use radon transform to compute the DFT along radial lines in the 2D-DFT plane
 - ▶ Projection MRI is similar, directly acquire DFT samples along radial lines
 - ▶ parallel lines is most common type of CT, other geometries also used.
- ▶ Given 22x256 data points of 2D-DFT of the image, need to compute the 256x256 image

Limitation of zero-filling

- ▶ A traditional solution: zero filling + I-DFT
 - ▶ set the unknown DFT coeff's to zero, take I-DFT
 - ▶ not good: leads to spatial aliasing
- ▶ Zero-filling is the minimum energy (2-norm) solution, i.e. it solves $\min_x \|x\|_2$ s.t. $y = Ax$. Reason
 - ▶ clearly, min energy solution in DFT domain is to set all unknown coefficients to zero, i.e. zero-fill
 - ▶ (energy in signal) = (energy in DFT)* 2π , so min energy solution in DFT domain is also the min energy solution
- ▶ The min energy solution will not be sparse because 2-norm is not sparsity promoting
 - ▶ In fact it will not be sparse in any other ortho basis either because $\|x\|_2 = \|\Phi x\|_2$ for any orthonormal Φ . Thus min energy solution is also min energy solution in Φ basis and thus is not sparse in Φ basis either
- ▶ But most natural images, including medical images, are approximately sparse (or are sparse in some basis)

Sparsity in natural signals/images

- ▶ Most natural images, including medical images, are approximately sparse (or are sparse in some basis)
 - ▶ e.g. angiograms are sparse
 - ▶ brain images are well-approx by piecewise constant functions (gradient is sparse): sparse in TV norm
 - ▶ brain, cardiac, larynx images are approx. piecewise smooth: wavelet sparse
- ▶ Sparsity is what lossy data compression relies on: JPEG-2000 uses wavelet sparsity, JPEG uses DCT sparsity
- ▶ But first acquire all the data, then compress (throw away data)
- ▶ In MRI or CT, we are just acquiring less data to begin with - can we still achieve exact/accurate reconstruction?

Use sparsity as a regularizer

- ▶ Min energy solution $\min_x \|x\|_2$ s.t. $y = Ax$ is not sparse, but is easy to compute $\hat{x} = A'(AA')^{-1}y$
- ▶ Can we try to find the min sparsity solution, i.e. find $\min_x \|x\|_0$ s.t. $y = Ax$
- ▶ Claim: If true signal, x_0 , is exactly S -sparse, this will have a unique solution that is EXACTLY equal to x_0 if $\text{spark}(A) > 2S$
 - ▶ $\text{spark}(A)$ = smallest number of columns of A that are linearly dependent.
 - ▶ in other words, any set of $(\text{spark}-1)$ columns are always linearly independent
- ▶ proof in class
- ▶ Even when x is approx-sparse this will give a good solution
- ▶ But finding the solution requires a combinatorial search:
 $O(\sum_{k=1}^S \binom{m}{k}) = O(m^S)$

- ▶ Basis Pursuit: replace ℓ_0 norm by ℓ_1 norm: closest norm to ℓ_0 that is convex

$$\min_x \|x\|_1 \text{ s.t. } y = Ax$$

- ▶ Greedy algorithms: Matching Pursuit, Orthogonal MP
- ▶ Key idea: all these methods “work” if columns of A are sufficiently “incoherent”
- ▶ “work”: give exact reconstruction for exactly sparse signals and zero noise, give small error recon for approx. sparse (compressible) signals or noisy measurements

Compressive Sensing

- ▶ name: instead of capturing entire signal/image and then compressing, can we just acquire less data?
- ▶ i.e. can we compressively sense?
- ▶ MRI (or CT): data acquired one line of Fourier projections at a time (or random transform samples at one angle at a time)
- ▶ if need less data: faster scan time
- ▶ new technologies that use CS idea:
 - ▶ single-pixel camera,
 - ▶ A-to-D: take random samples in time: works when signal is Fourier sparse
 - ▶ imaging by random convolution
 - ▶ decoding “sparse” channel transmission errors.
- ▶ Main contribution of CS: theoretical results

General form of Compressive Sensing

- ▶ Assume that an N -length signal, z , is S -sparse in the basis Φ , i.e. $z = \Phi x$ and x is S -sparse.
- ▶ We sense

$$y := \Psi z = \underbrace{\Psi \Phi}_{A} x$$

- ▶ It is assumed that Ψ is “incoherent w.r.t. Φ ”
 - ▶ or that $A := \Psi \Phi$ is “incoherent”
- ▶ Find x , and hence $z = \Phi x$, by solving

$$\min_x \|x\|_1 \text{ s.t. } y = Ax$$

- ▶ A random Gaussian matrix, Ψ , is “incoherent” w.h.p for S -sparse signals if it contains $O(S \log N)$ rows
- ▶ And it is also incoherent w.r.t. any orthogonal basis, Φ w.h.p. This is because if Ψ is r-G, then $\Psi \Phi$ is also r-G (ϕ any orthonormal matrix).
- ▶ Same property for random Bernoulli.

Quantifying “incoherence”

- ▶ Rows of A need to be “dense”, i.e. need to be computing a “global transform” of x .
- ▶ Mutual coherence parameter, $\mu := \max_{i \neq j} |A_i' A_j| / \|A_i\|_2 \|A_j\|_2$
- ▶ $\text{spark}(A)$ = smallest number of columns of A that are linearly dependent.
- ▶ Or, any set of $(\text{spark}(A) - 1)$ columns of A are always linearly independent.
- ▶ RIP, ROP
- ▶ many newer approaches...

Quantifying “incoherence”: RIP

- ▶ A $K \times N$ matrix, A satisfies the S -Restricted Isometry Property if constant δ_S defined below is positive.
- ▶ Let A_T , $T \subset \{1, 2, \dots, N\}$ be the sub-matrix obtained by extracting the columns of A corresponding to the indices in T . Then δ_S is the smallest real number s.t.

$$(1 - \delta_S)\|c\|^2 \leq \|A_T c\|^2 \leq (1 + \delta_S)\|c\|^2$$

for all subsets $T \subset \{1, 2, \dots, N\}$ of size $|T| \leq S$ and for all $c \in \mathbb{R}^{|T|}$.

- ▶ In other words, every set of S or less columns of A has singular values b/w $\sqrt{1 \pm \delta_S}$
- ▶ \Leftrightarrow every set of S or less columns of A approximately orthogonal
- ▶ $\Leftrightarrow A$ is approximately orthogonal for any S -sparse vector, c .

Examples of RIP

- ▶ If A is a random Gaussian, random Bernoulli, or Partial Fourier matrix with about $O(S \log N)$ rows, it will satisfy RIP(S) w.h.p.
- ▶ Partial Fourier * Wavelet: somewhat “incoherent”

Use for spectral estimation and comparison with MUSIC

- ▶ Given a periodic signal with period N that is a sparse sum of S sinusoids, i.e.

$$x[n] = \sum_k X[k] e^{j2\pi kn/N}$$

where the DFT vector, X , is a $2S$ -sparse vector.

- ▶ In other words, $x[n]$ does not contain sinusoids at arbitrary frequencies (as allowed by MUSIC), but only contains harmonics of $2\pi/N$ and the fundamental period N is known.
- ▶ In matrix form, $x = F^* X$ where F is the DFT matrix and $F^{-1} = F^*$.

- ▶ Suppose we only receive samples of $x[n]$ at random times, i.e. we receive $y = Hx$ where H is an “undersampling matrix” (exactly one 1 in each row and at most one 1 in each column)
- ▶ With random time samples it is not possible to compute covariance of $\underline{x}[n] := [x[n], x[n-1], \dots, x[n-M]]'$, so cannot use MUSIC or the other standard spectral estimation methods.
- ▶ But can use CS. We are given $y = HF^*X$ and we know X is sparse. Also, $A := HF^*$ is the conjugate of the partial Fourier matrix and thus satisfies RIP w.h.p.
- ▶ If have $O(S \log N)$ random samples, we can find X exactly by solving

$$\min_X \|X\|_1 \text{ s.t. } y = HF^*X$$

Quantifying “incoherence”: ROP

- ▶ θ_{S_1, S_2} : measures the angle b/w subspaces spanned by A_{T_1}, A_{T_2} for disjoint sets, T_1, T_2 of sizes less than/equal to S_1, S_2 respectively
- ▶ θ_{S_1, S_2} is the smallest real number such that

$$|c_1' A_{T_1}' A_{T_2} c_2| < \theta_{S_1, S_2} \|c_1\| \|c_2\|$$

for all c_1, c_2 and all sets T_1 with $|T_1| \leq S_1$ and all sets T_2 with $|T_2| \leq S_2$

- ▶ In other words

$$\theta_{S_1, S_2} = \min_{T_1, T_2: |T_1| \leq S_1, |T_2| \leq S_2} \min_{c_1, c_2} \frac{|c_1' A_{T_1}' A_{T_2} c_2|}{\|c_1\| \|c_2\|}$$

- ▶ Can show that δ_S is non-decreasing in S , θ is non-decreasing in S_1, S_2
- ▶ Also $\theta_{S_1, S_2} \leq \delta_{S_1 + S_2}$
- ▶ Also, $\|A_{T_1}' A_{T_2}\| \leq \theta_{|T_1|, |T_2|}$

Theoretical Results

- ▶ If x is S -sparse, $y = Ax$, and if $\delta_S + \theta_{S,2S} < 1$, then basis pursuit exactly recovers x
- ▶ If x is S -sparse, $y = Ax + w$ with $\|w\|_2 \leq \epsilon$, and $\delta_{2S} < (\sqrt{2} - 1)$, then solution of basis-pursuit-noisy, \hat{x} satisfies

$$\|x - \hat{x}\| \leq C_1(\delta_{2S})\epsilon$$

- ▶ basis-pursuit-noisy:

$$\min_x \|x\|_1 \text{ s.t. } \|y - Ax\|_2 \leq \epsilon$$

MP and OMP

DSP applications

- ▶ Fourier sparse signals
 - ▶ Random sample in time
 - ▶ Random demodulator + integrator + uniform sample with low rate A-to-D
- ▶ N length signal that is sparse in any given basis Φ
 - ▶ Circularly convolve with an N -tap all-pass filter with random phase
 - ▶ Random sample in time or use random demodulator architecture

Compressibility: one definition

- ▶ Decoding by Linear Programming (CS without noise, sparse signals)
- ▶ Dantzig Selector (CS with noise)
- ▶ Near Optimal Signal Recovery (CS for compressible signals)
- ▶ Applications of interest for DSP
 - ▶ Beyond Nyquist:... Tropp et al
 - ▶ Sparse MRI: ... Lustig et al
 - ▶ Single pixel camera: Rice, Baranuik's group
 - ▶ Compressive sampling by random convolution : Romberg

Sparse Recon. with Partial Support Knowledge

- ▶ Modified-CS (our group's work)
- ▶ Weighted ℓ_1
- ▶ von-Borries et al

Treating Outliers as Sparse Vectors

- ▶ Dense Error Correction via ℓ_1 minimization
- ▶ “Robust” PCA
- ▶ Recursive “Robust” PCA (our group’s work)